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Handheld chromatic pupillometry can accurately and rapidly reveal functional loss in glaucoma

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ABSTRACT

Background/aims Early detection and treatment of glaucoma can delay vision loss. In this study, we evaluate the performance of handheld chromatic pupillometry (HCP) for the objective and rapid detection of functional loss in glaucoma.

Methods In this clinic-based, prospective study, we enrolled 149 patients (median (IQR) years: 68.5 (13.6) years) with confirmed glaucoma and 173 healthy controls (55.2 (26.7) years). Changes in pupil size in response to 9 s of exponentially increasing blue (469 nm) and red (640 nm) light-stimuli were assessed monocularly using a custom-built handheld pupillometer. Pupillometric features were extracted from individual traces and compared between groups. Features with the highest classification potential, selected using a gradient boosting machine technique, were incorporated into a generalised linear model for glaucoma classification. Receiver operating characteristic curve analyses (ROC) were used to compare the performance of HCP, optical coherence tomography (OCT) and Humphrey Visual Field (HVF).

Results Pupillary light responses were altered in glaucoma compared with controls. For glaucoma classification, HCP yielded an area under the ROC curve (AUC) of 0.94 (95% CI 0.91 to 0.96), a sensitivity of 87.9% and specificity of 88.4%. The classification performance of HCP in early-moderate glaucoma (visual field mean deviation (VFMD) > -12 dB; AUC=0.91 (95% CI 0.87 to 0.95)) was similar to HVF (AUC=0.91) and reduced compared with OCT (AUC=0.97; p=0.01). For severe glaucoma (VFMD ≤ -12 dB), HCP had an excellent classification performance (AUC=0.98, 95% CI 0.97 to 1) that was similar to HVF and OCT.

Conclusion HCP allows for an accurate, objective and rapid detection of functional loss in glaucomatous eyes of different severities.

INTRODUCTION

Early detection and treatment of glaucoma can delay vision loss and consequently alleviate the health economic burden associated with the condition.^{1 2} However, glaucoma is often diagnosed at a late stage, especially in some low-income and middle-income countries, where up to 50% of patients are already blind in one eye at presentation.^{3 4}

The detection of glaucoma is challenging, in part because no standalone, affordable and accurate tool allows for it in an opportunistic or community

setting. Existing methods, like optical coherence tomography (OCT) and standard automated perimetry (SAP) require expensive and highly calibrated apparatus. Furthermore, SAP is subjective, demanding in time and effort and does not always reflect the severity of structural decrements observed in early-stage glaucoma.^{5 6}

Chromatic pupillometry, which measures the pupillary responses to light stimulations of different wavelengths, has become increasingly recognised as an effective method for evaluating retinal and optic nerve health.⁷ This technique investigates the integrity of retinal photoreceptors (ie, rods, cones and intrinsically photosensitive retinal ganglion cells (ipRGCs)) which contribute differentially to the pupillary light response (PLR).^{8–10} ipRGCs are a subset of RGCs that are intrinsically photosensitive,⁸ and also integrate input from the outer retina, to mediate the PLR.¹⁰

Recent findings from our group and others suggest that ipRGC loss or dysfunction occurs in glaucoma, even at the earliest stages, resulting in abnormal pupillary responses to full-field or sectorial chromatic stimuli.^{11–13} In addition, multifocal stimuli targeting both subcortical (ie, ipRGC-driven responses) and adjacent corticopretectal (ie, originating from M-cones and L-cones through RGCs) chromatic pupillary responses, have been suggested to offer a higher sensitivity to glaucomatous functional alterations.^{14 15} Although chromatic pupillometry demonstrates high efficacy in the detection of functional abnormalities in glaucoma, the used lab-based devices are commonly bulky, expensive and unsuitable for everyday clinical use.

Using a custom-built handheld pupillometer, in this study, we evaluated the pupillary responses to exponentially increasing blue and red light stimulations in patients with different severities of glaucoma. Furthermore, we compared the performance of our handheld chromatic pupillometer (HCP) for glaucoma classification with established structural (ie, OCT) and functional (ie, SAP) investigation tools.

MATERIALS AND METHODS

Participants

Patients with unilateral or bilateral glaucoma and healthy controls were included in this clinic-based, cross-sectional study conducted between June 2017 and November 2018 (figure 1). In this prospective study, data collection was planned before pupillometric assessments and reference standard

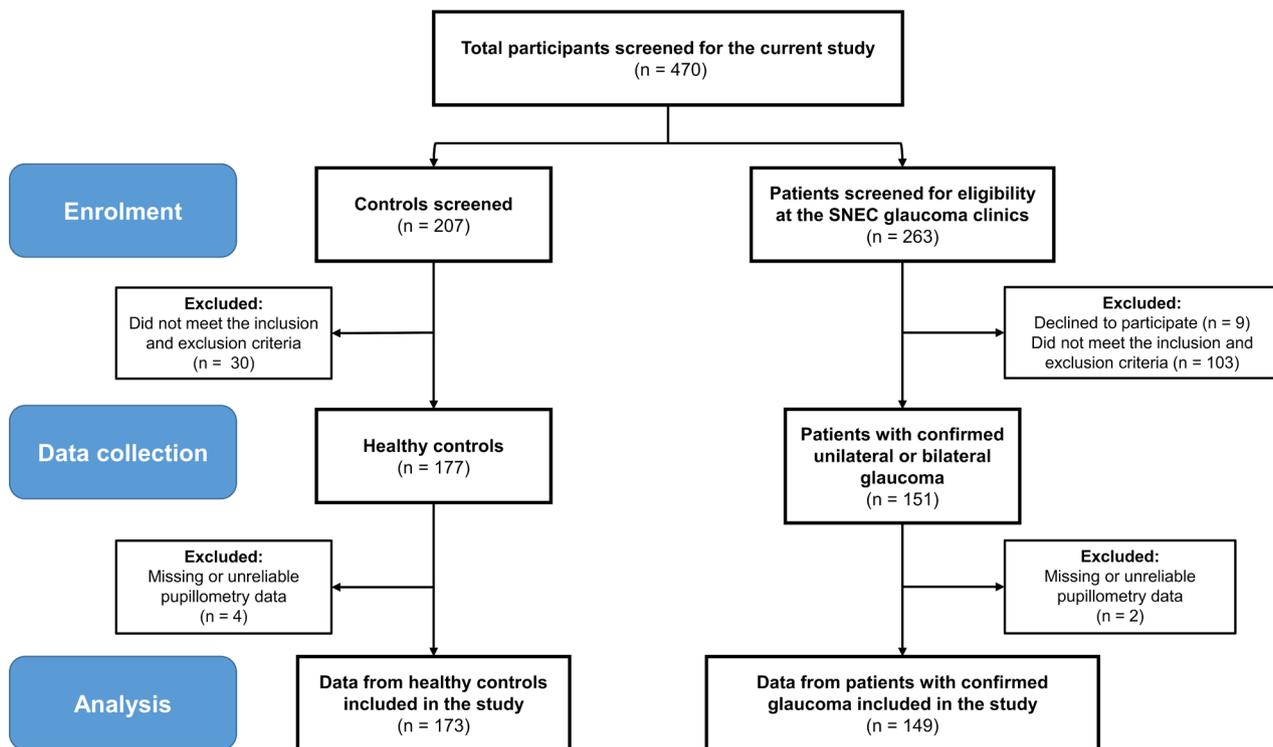


Figure 1 Diagram showing the flow of enrolment and exclusion of patients and data. A total of 470 participants including 207 controls and 263 patients were screened for this study. Out of the control group, 30 participants did not meet the study's inclusion and exclusion criteria and the pupillometry data collected from four control participants were unreliable (n=2) or missing (n=2). Out of 263 patients screened at the Singapore National Eye Centre (SNEC) glaucoma clinics, 9 declined to participate and 103 did not meet the study's inclusion and exclusion criteria. The pupillometry data collected from two glaucoma patients were missing or unreliable. This study included the data from 173 controls and 149 patients with confirmed unilateral or bilateral glaucoma.

confirmation. Glaucoma patients were recruited consecutively from the glaucoma clinics of glaucoma specialists AT and RH at the Singapore National Eye Centre (SNEC). Control participants were recruited from the general clinics of the hospital. All participants underwent a comprehensive ophthalmological evaluation (details in online supplemental methods 1). Controls were defined as subjects with no glaucomatous optic neuropathy (intraocular pressure less than 21 mm Hg, open iridocorneal angles (on gonioscopy) in all quadrants, healthy optic nerves and normal visual fields (VF)). Patients with clinically confirmed glaucoma were diagnosed by a fellowship trained specialist by the presence of glaucomatous optic neuropathy (loss of neuroretinal rim with a vertical cup-disc ratio of >0.7 and/or notching with nerve fibre layer defect attributable to glaucoma) with compatible VF defect. Based on Hodapp-Parish-Anderson's criteria, patients were separated into early-moderate-stage (VF mean deviation (VFMD) scores better than -12 dB) and severe-stage (VFMD scores of -12 dB or worse) groups.¹⁶ This grouping was adopted to evaluate the performance of HCP in patients with less perceptible VF loss (early-moderate) and patients with severe glaucoma who are at highest risk for rapid worsening of the disease, lifetime blindness and deterioration of quality of life.¹⁷

Were also excluded patients with: (1) an unconfirmed glaucoma diagnosis or any associated ophthalmic conditions such as other causes of optic neuropathy, retinopathies and/or ocular motor disorders; (2) clinically significant pupillary abnormalities except for relative afferent pupillary defects (RAPD) in the glaucoma group; (3) clinically diagnosed psychiatric or neurological disorders, including dementia and (4) patients who had

undergone intraocular surgery within the past 6 months, had severe ocular trauma or were using psychotropic or other medications known to affect the pupillary control pathways. Written informed consent was obtained from all participants. Research procedures adhered to ethical principles outlined in the Declaration of Helsinki. The full study protocol is available from the corresponding author on reasonable request.

Handheld chromatic pupillometry

Dynamic pupillary responses to chromatic stimulations in patients and controls were evaluated without dark adaptation using a custom-built handheld pupillometer in dimly-lit rooms (<3 lux). A detailed description of the device and light calibration is provided in online supplemental methods 2, online supplemental figure 1. Experimenters were masked to the clinical information and final diagnosis of the participant during data acquisition.

Each participant underwent a 1 min pupillometric self-examination that consisted of the following steps: 10 s of darkness (baseline pupil measurement); 9 s of exposure to exponentially-increasing blue light (11.7 – 14.4 log photons/cm²/s; peak wavelength (λ_{\max})= 469 nm, full width at half maximum (FWHM)= 33 nm); 22 s of darkness to assess the dynamics of pupillary redilation to baseline; exposure to 9 s exponentially increasing red light stimulus (11.9 – 14.3 log photons/cm²/s; λ_{\max} = 640 nm, FWHM= 17 nm); 10 s of darkness to assess pupillary redilation (figure 2A). Light stimulations covered 50° of the VF without considering reflections off the interior of the device. Participants were requested to fixate a central dim red zone (<0.1 lux)

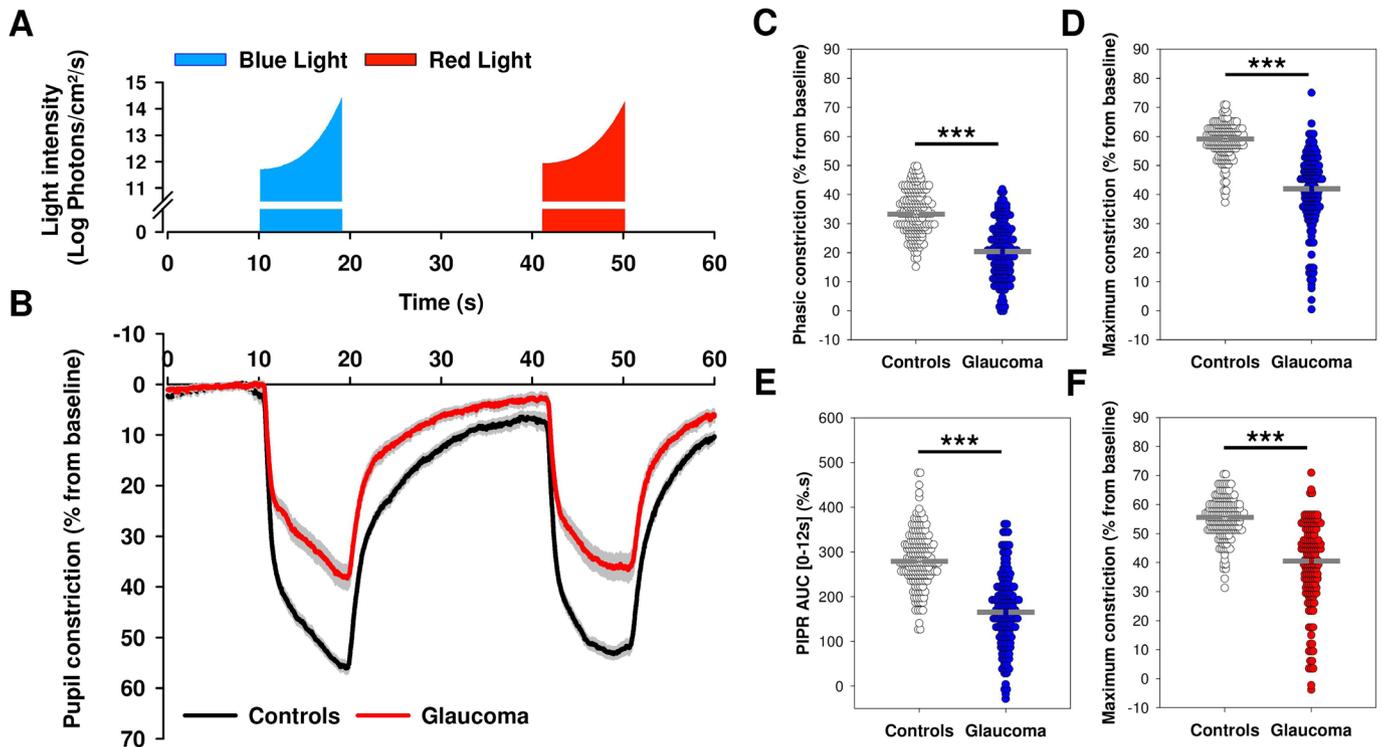


Figure 2 Average baseline-adjusted pupillary responses to the 1 min light paradigm in patients with glaucoma and controls. (A) After onset, light stimuli intensity increased exponentially from 11.7 to 14.4 log photons/cm²/s for blue light and from 11.9 to 14.3 log photons/cm²/s for red light. The duration of both blue and red light exposures was 9 s. Blue light stimulus onset was preceded by 10 s of darkness to quantify baseline pupil size and followed by 22 s of darkness to assess pupillary redilation prior to red light onset. Red light was followed by 10 s of darkness to assess the pupil's redilation process. (B) Baseline-adjusted pupil constriction increased (pupil size decreased) rapidly at light onset and progressively as a function of the gradually increasing light exposure. In comparison to controls, patients with glaucoma exhibited significant alterations in the pupillary light responses. Data are plotted as average \pm SE. (C–F) Dot plots representing differences in main pupillometric features in response to blue (C, D, E) and red (F) lights in patients with glaucoma compared with controls. The median of each group is represented as a dashed grey line. Statistical comparisons between groups were performed using a Mann-Whitney U test. *** $p < 0.001$. AUC, area under the curve; PIPR, post-illumination pupillary response.

delivered using a red, green, blue (RGB) light-emitting diode (LED). Light was administered to the study eye, with the fellow eye covered by the participant's hand. In controls and patients with bilateral glaucoma and two eligible eyes, the study eye was selected randomly by coin toss.

Data analysis and statistics

Horizontal pupil radius measurements were individually processed using a semiautomated algorithm for blink artefact removal and expressed as a percentage change from baseline pupil size (figure 2B). This baseline correction accounted for any differences in baseline pupil size between participants and across groups. Sixteen principal pupillometric features were extracted from individual blink-free traces (online supplemental table 1).

Pupillometric features are presented as median (IQR) and were compared between controls and glaucoma groups using a Mann-Whitney U test. Demographics and ophthalmological examination outcomes are represented as median (IQR) and were compared between controls and glaucoma groups using a non-parametric Mann-Whitney U test or a χ^2 test, and between controls and the different glaucoma severity groups using a Kruskal-Wallis One-Way analysis of variance on Ranks. Post hoc analysis was done pairwise using Dunn's method.

The relative contribution of demographic (age, gender and ethnicity), clinical (diabetes status) and pupillometric

features in the training of the glaucoma classification model was determined using a gradient boosting machine (GBM) technique. A GBM is an ensemble of simple decision trees grown sequentially. The more a feature is associated with an improvement of the classification performance, the higher its relative contribution to the model. Top pupillometric contributing features (ie, excluding age, gender, ethnicity and diabetes status), corresponding to a cumulative relative contribution of at least 90% were used in a generalised linear model (GLM), a binary logistic regression that estimated the relationship between the outcome (no glaucoma/glaucoma) and continuous independent variables (pupillometric features). Adjusted ORs (adj. ORs) for pupillometric variables as well as their significance (Wald's test) were calculated. The classification performance of the GLM's fitted values (ie, glaucoma probability scores) was determined using a receiver operating characteristic curve (ROC) analysis. The area under the ROC curve (AUC), sensitivity, specificity, accuracy, positive and negative predictive values (PPV and NPV) were calculated at best statistical cut-off (highest Youden's J). Accuracy, PPV and NPV took into account a glaucoma prevalence of 3.54% in the general population (40–80 years old).¹⁸ Similar analytical approaches were used for OCT and Humphrey VF (HVF) features. The Akaike information criterion (AIC) was used as an indicator of the models' relative quality. Clinical diagnoses established on the same day as HCP by a fellowship trained specialist with

Table 1 Demographics and clinical characteristics of the study eye in controls and patients with glaucoma

	Controls	Glaucoma		
		Early-moderate glaucoma	Severe glaucoma	All glaucoma
N	173	96	53	149
Age (years) [¶]	55.2 (26.7)	68.5 (14.2)***	68.3 (14.3)***	68.5 (13.6)***
Gender, no (% male)*	80/173 (46.2)	56/96 (58.3)‡	43/53 (81.1)***	99/149 (66.4)***
Ethnicity, no (% Chinese)*	157/173 (90.8)	91/96 (94.8)§	39/53 (73.6)**	130/149 (87.2)
Family history of glaucoma, no (%)*	5/173 (2.9)	23/96 (24.0)***	9/53 (17.0)***	32/149 (21.5)***
Diabetes, no (% with)*	15/173 (8.7)	25/96 (26.0)***	14/53 (26.4)***	39/149 (26.2)***
Cataract, no (% with)*	46/173 (26.6)	55/96 (57.3)***	33/53 (62.3)***	88/149 (59.1)***
PCIOL, no (% with)*	4/173 (2.3)	30/96 (31.3)***	18/53 (34.0)***	48/149 (32.2)***
SE, median (IQR), D [¶]	-1.6 (3.9)	-1.1 (4.9)	-0.8 (3.8)	-0.9 (4.4)
BCVA, median (IQR), LogMar [¶]	0.08 (0.2)	0.1 (0.2)*** †	0.3 (0.3)***	0.2 (0.2)***
VCDR, median (IQR) [¶]	0.40 (0.20)	0.80 (0.15)*** †	0.90 (0.10)***	0.80 (0.10)***
VFMD, median (IQR), dB [¶]	-1.0 (2.1)	-4.7 (5.4)*** §	-18.6 (9.6)***	-8.7 (10.6)***
PSD, median (IQR), dB [¶]	1.6 (0.7)	4.5 (5.3)*** §	11.1 (4.5)***	7.7 (7.4)***
VFI, median (IQR), % [¶]	99.0 (2.3)	90.0 (14.0)*** §	51.5 (32.8)***	79.5 (30.5)***
Mean RNFL thickness, median (IQR), µm [¶]	97.0 (11.0)	72.0 (15.0)*** ‡	58.0 (10.5)***	68.0 (18.8)***
RNFL symmetry, median (IQR), % [¶]	86.5 (13.0)	61.0 (37.0)*** †	40.5 (43.5)***	52.0 (43.0)***
Rim area, median (IQR), mm ² [¶]	1.31 (0.27)	0.80 (0.29)***	0.69 (0.27)***	0.75 (0.31)***

A Kruskal-Wallis one way ANOVA on ranks was used to compare controls, early-moderate stage and severe stage glaucoma groups. A post-hoc pairwise comparison between the 3 groups was done using Dunn's method. Difference between groups is indicated as ** p<0.01; *** p<0.001 for comparison with controls, and † p<0.05; ‡ p<0.01; § p<0.001 for pairwise comparison between early-moderate and severe glaucoma. [¶] Statistics done using a Mann Whitney U-test between controls and all glaucoma group. * Statistics done using a χ^2 test. ANOVA, analysis of variance; BCVA, best-corrected visual acuity; HVF, Humphrey visual field; LogMar, logarithm of minimum angle of resolution; PCIOL, posterior chamber intra-ocular lens; PSD, pattern SD; RNFL, retinal nerve fibre layer; SE, spherical equivalent; VCDR, vertical cup disk ratio; VFI, Visual Field Index; VFMD, visual field mean deviation.

access to participants' clinical records were used as reference standard. Pairwise comparison between the AUCs of HCP, OCT and HVF was performed using DeLong's method with Bonferroni correction. Machine learning and statistical procedures were performed using R V.3.6.3: A Language and Environment for Statistical Computing (R Core Team, Vienna, Austria). Figures were plotted using Sigmaplot V.14.0 (Systat Software, San Jose, California, USA). Intended sample size calculation is provided in online supplemental methods 3.

RESULTS

Participants

A total of 470 participants were screened to take part in this study including 207 potential controls and 263 patients from the SNEC clinics. Of these, 142 participants did not meet the inclusion criteria of this study and the data of 6 participants (4 controls, 2 glaucoma) were excluded due to unreliable or missing pupillometry traces (figure 1). The data from 173 healthy controls (median age 55.2 (26.7) years, 46.2% males, 90.8% ethnic-Chinese) and 149 patients (68.5 (13.6) years, 66.4% males, 87.2% ethnic-Chinese) with bilateral or unilateral glaucoma were included in this study. The glaucoma group included 119 patients with primary open angle glaucoma (75 with high tension glaucoma and 44 with normal tension glaucoma), 27 patients with primary angle closure glaucoma and 3 patients with other glaucoma subtypes (1 pseudophakic, 1 pseudoexfoliation and 1 pigment dispersion glaucoma). Glaucoma patients were further divided into early-moderate and severe glaucoma groups. A detailed description of the demographics and clinical characteristics of all groups is provided in table 1. No

adverse events were reported from any of the procedures used in the study.

Pupillary responses to blue and red lights are altered in patients with glaucoma

Baseline pupil size was reduced in patients with glaucoma compared with controls ($U=7302.0$, $p<0.001$) (online supplemental table 2). In both groups, the pupil, respectively, constricted in a phasic (fast) then gradual manner in response to the onset and exponential increase of the light stimuli (figure 2A,B). The average pupillary constriction curves were, however, markedly altered in the glaucoma group compared with controls (figure 2B). Multiple PLR features were different between groups. Principally, phasic constriction to blue ($U=3905$; $p<0.001$) and red ($U=4258$; $p<0.001$) lights, as well as maximum constriction to blue ($U=1912.5$; $p<0.001$) and red ($U=3406.5$; $p<0.001$) lights were reduced in patients with glaucoma (figure 2C, D and F; online supplemental table 2). Pupillary redilation was also affected by glaucoma as the area under the redilation curve after blue light offset (PIPR AUC 0–12 s) (figure 2E), the post-illumination pupillary responses 6 s after blue or red light offset (PIPR6s), as well as their difference (Net PIPR6s), were reduced in glaucomatous eyes (all, $p<0.001$, online supplemental table 2).

Relative feature contribution and classification performance of HCP for glaucoma

The GBM analysis on 16 pupillometric features in addition to age, gender, ethnicity and diabetes status evaluated the importance of pupillometric and demographic variables in

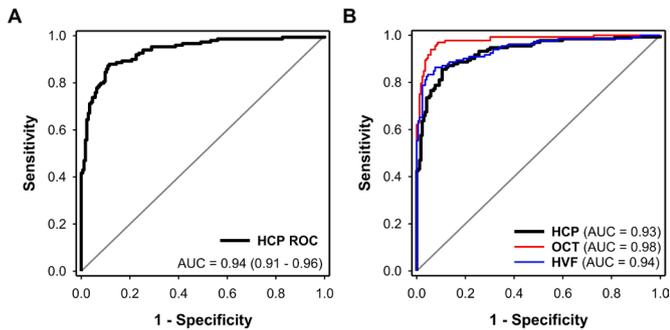


Figure 3 Receiver operating characteristic (ROC) curves reflecting the classification performance of HCP, OCT and HVF. (A) Receiver operating characteristic curve of HCP in 173 controls and 149 patients with glaucoma. The AUC of HCP was 0.94 (95% CI 0.91 to 0.96). (B) ROC curves of HCP, HVF and OCT in a similar population of 172 controls and 132 glaucoma patients. The AUC of HCP for the classification of glaucoma was 0.93 (0.90–0.96) and was similar to that of HVF (0.94 (0.92–0.97); $p=0.56$) but reduced compared with OCT (0.98 (0.96–0.99); $p=0.005$). The AUC of HVF was significantly lower than OCT ($p=0.02$). AUC, area under the curve; HCP, handheld chromatic pupillometry; HVF, Humphrey Visual Field; OCT, optical coherence tomography.

training the glaucoma classification model (online supplemental figure 2). The variable with the highest contribution to the classification model was maximum constriction to blue light (62.2% relative contribution), followed by PIPR AUC 0–12 s and maximum constriction to red light with relative contributions of 7.3% and 6.3%, respectively. Age and gender contributed 1.4% and 1.1% to the model, respectively, while the relative contributions of diabetes-status and ethnicity were negligible (0%–0.1%) (online supplemental figure 2). Using top-contributing pupillometric features and excluding age, gender, ethnicity as well as diabetes status, we developed a GLM for glaucoma classification. The GLM (AIC=226.8) had an AUC of 0.94 (0.91–0.96), a sensitivity of 87.9% (81.6%–92.7%) and a specificity of 88.4% (82.7%–92.8%) (figure 3A). Significant variables in this model were maximum constriction to blue light ($p=0.002$) with an adj. OR of 0.21 (0.08–0.56) per 10% increase in constriction and constriction latency to blue light ($p=0.05$) with an adj. OR of 1.41 (1.00–1.98) per 100 ms increase in latency. To ensure that overfitting did not affect our results, we validated our model using a 10-fold cross validation approach. The cross-validated AUC of the GLM was 0.93 (0.90–0.96). Detailed classification performance and cross-tabulation results are shown in online supplemental table 3. Interestingly, if maximum pupillary constriction to blue light was missing/removed from the model (eg, due to blinks or other artefacts), a GLM developed on the eight remaining pupillometric features, still maintains high classification performance (AUC=0.93, 95% CI 0.90 to 0.96) with significant variables becoming PIPR AUC 0–12 s ($p<0.001$, adj. OR of 0.80 (0.71 - 0.91) per increase of 10%.s in the variable), maximum constriction to red light ($p<0.001$, adj. OR of 0.41 (0.25 - 0.69) per increase of 10% in in the variable), constriction latency to blue light ($p=0.04$, adj. OR of 1.40 (1.01 - 1.93) per increase of 100 ms in the variable), and constriction latency to red light ($p=0.02$, adj. OR of 1.06 (1.01 - 1.11) per increase of 100 ms in the variable).

The exact statistical powers for the calculation of sensitivity and specificity of HCP were 96.5% and 97.2% for $\alpha=0.05$

Table 2 Comparison of the classification performance of HCP, OCT and HVF in a population of controls (n=172) and patients with glaucoma

	HCP	OCT	HVF
All glaucoma (n=132)			
AUC	0.93 (0.90 to 0.96)	0.98 (0.96 to 0.99)*	0.94 (0.92 to 0.97)†
Sensitivity, %	85.6 (78.4 to 91.1)	97.0 (92.4 to 99.2)	86.4 (79.3 to 91.7)
Specificity, %	89.5 (84.0 to 93.7)	91.3 (86.0 to 95.0)	92.4 (87.4 to 95.9)
PPV, %‡	23.1 (16.2 to 31.9)	29.0 (20.1 to 39.9)	29.5 (19.8 to 41.5)
NPV, %‡	99.4 (99.1 to 99.6)	99.9 (99.7 to 1)	99.5 (99.2 to 99.7)
Accuracy, %‡	89.4 (85.4 to 92.6)	91.5 (87.8 to 94.3)	92.2 (88.6 to 95.0)
Early-moderate glaucoma (n=87)			
AUC	0.91 (0.87 to 0.95)	0.97 (0.95 to 0.99)*	0.91 (0.87 to 0.96)†
Sensitivity, %	81.6 (71.9 to 89.1)	95.4 (88.6 to 98.7)	79.3 (69.3 to 87.3)
Specificity, %	90.1 (84.6 to 94.1)	92.4 (87.4 to 95.9)	92.4 (87.4 to 95.9)
Severe glaucoma (n=45)			
AUC	0.98 (0.97 to 1)	1 (1 to 1)	1 (1 to 1)
Sensitivity, %	95.6 (84.9 to 99.5)	100 (92.1 to 100)	100 (92.1 to 100)
Specificity, %	94.2 (89.6 to 97.2)	97.7 (94.2 to 99.4)	100 (97.9 to 100)

Data are represented as average (95% CI). The statistical pairwise comparison of AUCs was performed using DeLong's method.

* $p<0.05$ between HCP and OCT, after Bonferroni correction.

† $p<0.05$ between HVF and OCT, after Bonferroni correction.

‡Values calculated at a disease prevalence of 3.54%.

AUC, area under the curve; HCP, handheld chromatic pupillometry; HVF, Humphrey Visual Field; NPV, negative predictive value; OCT, optical coherence tomography; PPV, positive predictive value.

at the disease prevalence of 46% observed in the final sample (n=322).

Comparison of performance characteristics between HCP, OCT and HVF

Using a subgroup of patients and controls with no missing OCT and HVF variables (172 controls; 132 glaucoma) we adopted the same GBM approach and developed GLMs for glaucoma classification using top contributing features of OCT (by order of importance: mean RNFL thickness, rim area, VCDR, RNFL symmetry) and HVF (by order of importance: VF Index, VFMD and pattern SD). The AIC's of the GLMs were 218.8, 117.3 and 180.8 for HCP, OCT and HVF, respectively. The AUC of HCP for the detection of glaucoma was 0.93 (0.90–0.96) and was similar to that of HVF (0.94 (0.92–0.97); $Z=-0.59$; $p=0.56$) but reduced compared with OCT (0.98 (0.96–0.99); $Z=-2.83$; $p=0.005$) (figure 3B, table 2). The AUC of HVF was significantly lower than OCT ($Z=2.42$; $p=0.02$) (figure 3B, table 2).

Classification performance of HCP in a subgroup of glaucoma patients and controls matched for age, diabetes and cataract surgery statuses

To further consolidate our findings, we performed a subgroup analysis after matching controls and glaucoma groups for age (controls: 66.3 (6.0) years; glaucoma: 68.0 (5.3) years; $U=1940.5$, $p=0.61$), diabetes ($\chi^2=1.36$, $p=0.25$) and cataract surgery ($\chi^2=0.43$, $p=0.51$) statuses. In this sample of 64 controls and 64 glaucoma patients, using a new GLM, the AUC of HCP remained high (0.93 (0.88–0.97)), while sensitivity was 92.2% and specificity 81.3%. The classification performance of HCP was not significantly different

from that of HVF (AUC=0.92, 95% CI 0.86 to 0.97) and OCT (AUC=0.97, 95% CI 0.95 to 1).

Classification performance of HCP across glaucoma severity groups

Alterations in the pupillary constriction profiles were dependent on the severity of glaucoma (online supplemental figure 3A). For example, maximum constriction to blue light gradually decreased with the severity of the disease ($H=182.4$, $p<0.001$; online supplemental figure 3B). Using specific GLMs developed using HCP features in controls and different sub-groups of glaucoma severity, the AUC of HCP for the detection of early-moderate stage glaucoma was 0.91 (0.87–0.95) and was similar to HVF (0.91 (0.87–0.96); $Z = -0.13$; $p=0.90$) and reduced compared with OCT (0.97 (0.95–0.99); $Z=-2.56$; $p=0.01$) (table 2). Conversely, the performance of HCP for the detection of severe glaucoma (AUC=0.98, 95% CI 0.97 to 1) was similar to OCT and HVF (table 2).

DISCUSSION

In this study, we demonstrate that pupillometric dysfunctions occur in glaucoma and can be revealed with a custom-built handheld pupillometer, delivering tailored, fast, chromatic light paradigms. Furthermore, a model including predominant pupillometric features of the disease can be used to detect functional glaucomatous loss with high accuracy.

The reactivity of the pupil to light is dependent on the integrity of retinal photoreceptors and their neural circuitry.¹⁹ We previously demonstrated that ramping-up chromatic light stimulations demonstrate reduced PLRs in different severities of glaucoma.¹¹ The method was subsequently shown not to be affected by mild and moderate cataracts or refractive errors,^{20,21} with the potential of detecting subtle functional deficits in eyes with early-stage glaucoma.¹³ Using a handheld pupillometer that delivers a similar, yet shortened and refined light paradigm, our study confirms altered PLRs in patients with glaucoma and underlines the effectiveness of direct, monocular, HCP for the detection of functional loss in the disease.

Our results show alterations in the ipRGC-driven pupillary response which are in agreement with electrophysiological reports in patients with glaucoma,²² and findings in rodent models of chronic ocular hypertension.²³ Interestingly, among the various pupillometric features altered in glaucomatous eyes, maximum constriction to blue light (14.4 log photons/cm²/s), and not the PIPR or Net PIPR,¹² showed the highest relative contribution to the classification performance of the GBM model. These findings suggest that the pupillometric hallmarks of ipRGC integrity are also dependent on the pattern of a light stimulation. In principle, our gradually increasing light stimulations evaluated the integrated extrinsic and intrinsic ipRGCs response,^{11,13} but would likely yield maximum intrinsic (ie, melanosin) stimulation and contribution at peak blue light intensity.⁸ In addition to RGC damage, electrophysiological and histological studies have also suggested alterations in outer retinal photoreception in glaucoma.^{24,25} Here, alterations in the latency and phasic pupillary constriction amplitudes, in addition to changes in the early redilation phases of the PIPR (<1.7 s) suggested to involve rods,²⁶ are in agreement with the aforementioned literature and suggest outer retinal dysfunction in glaucoma.

Findings from previous studies focusing on the RAPD were only moderately encouraging with AUCs ranging between 0.74 and 0.85.^{27–30} This was probably due to the reduced classification performance of RAPD features in symmetric glaucoma,²⁷

leading to the categorisation of pupillometers as devices with limited value for glaucoma detection. The performance characteristics of direct or consensual pupillometry for the detection of functional loss in glaucoma were also evaluated by multiple groups.^{12,14,31–34} Using the direct pupillary response to shape-like stimulations,³⁴ or consensual PIPR to quadrant stimulations,¹² pupillometry yielded high classification accuracy (AUCs >0.90) for glaucoma. Conversely, chromatic multifocal infrared pupillometry only showed fair to good diagnostic accuracy with AUCs ranging from 0.71 to 0.82 for the detection of mild and moderate to severe glaucoma, respectively.¹⁴ While these original approaches used differential spatial and multifocal stimulation of the retina, the studies had small sample sizes, and relied on devices that required good fixation and unfailing cooperation from patients. Using the RAPDx system (Konan Medical, California, USA), a 7 min stimulation sequence and an elaborate analytical strategy, Chang *et al* showed that the performance was lowest (AUC=0.78) when comparing results between eyes and increased (AUC=0.87) in a model including asymmetry in pupillometric outcomes and age.³⁵ With a similar analytical approach applied only to pupillometric features, in this proof-of-concept study, we show that a low-cost handheld pupillometer delivering short-duration light stimulations, requiring minimal fixation aptitudes and no dark-adaptation, can highlight functional loss in eyes with glaucoma. Similar fast pupillometry-based approaches are also showing promise for the fast detection of functional loss in other ocular conditions.³⁶

From an analytical standpoint, although only two pupillometric features were significant among nine to predict glaucoma using a GLM, keeping all the nine features would have practical interest. For instance, if a patient blinks at peak blue light intensity, the feature with the highest relative contribution, that is, maximum constriction to blue light, may become unreliable. Using the eight remaining pupillometric features (online supplemental figure 2) in a new GLM—potentially embedded in an analysis software—HCP can still detect functional loss in glaucoma with high accuracy (AUC of 0.93 (0.90–0.96) instead of 0.94 (0.91–0.96)). This approach could improve the reliability of a testing procedure, reduce administration time, and prevent the repetition of a test if artefacts such as blinks were to mask on one or more pupillometric features.

Glaucoma is a treatable disease, nonetheless the efficacy of a treatment is dependent on the severity of the condition at diagnosis.³⁷ In the USA, more than US\$2500/patient/year is spent on advanced glaucoma, compared with US\$623 on early glaucoma.³⁸ Nevertheless, the prevalence of undiagnosed and untreated glaucoma remains high in developed countries and alarmingly so in the developing world, reaching magnitudes over 95% in the rural parts of some countries.³⁹ Major advances in telemedicine and artificial intelligence, may yet reduce the cost of accurate glaucoma detection. Considering its high accuracy (89.4%) and NPV (>99%), and its promise to detect other sight threatening conditions,⁷ HCP's aptitudes for glaucoma detection should be investigated further in a dedicated screening setting (eg, community, general practitioner's clinic). Furthermore, at a fraction of the cost (ie, prototype excluding iOS system and software development costs at ~US\$450), its performance is similar to that of OCT and HVF in detecting severe glaucoma. Thus, HCP has the potential to alleviate burden of blindness on first presentation to glaucoma clinics in developing countries.³ Future studies should evaluate the potential of pupillometry in general and HCP in particular for the tracking of glaucoma progression.

Our study has some limitations, inherent to the novelty of this proof-of-concept investigation. First, it was performed in a clinical setting where the prevalence of glaucoma is higher than the community. Without a prospective community-based study, we are

therefore unable to infer whether HCP would yield similar diagnostic performance in a non-clinical setting or a less selected, multi-ethnic population with inherently different demographic and clinical characteristics. Second, given our intent to evaluate the performance of HCP in a busy and time-sensitive clinical setting, we did not dark-adapt or pharmacologically dilate the pupils of our participants. Therefore, while our method is likely to underestimate the absolute magnitude of PLRs in participants, our findings are all the more applicable in clinical, time-constrained settings. Third, abnormal PLRs may also be present in other ocular or even neurological conditions.^{7,40,41} Although that may decrease the specificity of HCP for glaucoma, the ability to uncover multiple ocular diseases is valuable for screening strategies.³

In conclusion, our proof-of-concept study highlights the feasibility and high accuracy of chromatic pupillometry delivered using a handheld device for the objective detection of functional loss in glaucoma in a clinical setting. Further community-based or opportunistic screening studies, as well as cost-effectiveness analyses, are necessary to confirm whether HCP is a useful tool for glaucoma screening.

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Competing interests DM has a patent application based on the pupillometry protocol used in the present study (PCT/SG2015/050494): A method and system for monitoring and/or assessing pupillary responses. RPN, TA and DM have a patent application based on the handheld pupillometer used in this study (PCT/SG2018/050204): Handheld ophthalmic and neurological screening device. The rest of the authors have no conflicts of interest to disclose.

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